

Microwave Subsurface Imaging of Living Tissues

G.M.Altshuller, K.P.Gaikovich, V.L.Vaks

Institute for Physics of Microstructures of RAS, Nizhny Novgorod, GSP-105, Russia,
603950. E-mail: vax@ipm.sci-nnov.ru; phone: (8312)675037; fax: (8312)675553.

A method of subsurface imaging of living tissues has been worked out. It is based on 2-D microwave reflectivity scanning using a small-aperture near-field contact antenna with the size of 1 cm as a probe (the same antenna was used in our near-field radiometry measurements [1]). This antenna consisted of two in-phase dipoles connected to a symmetric strip line operating as a matching resonator. The scheme of measurements is shown in Fig.1.

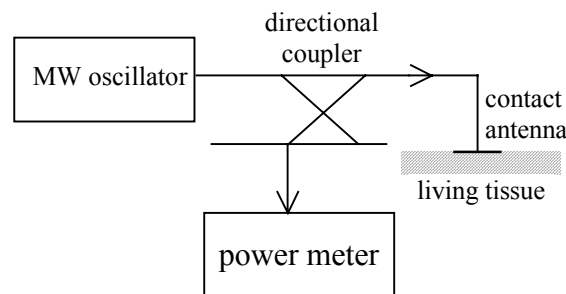


Fig.1. Measurements scheme.

As the probe moves along the tissue surface, the equivalent impedance has variations related to subsurface inhomogeneities. These variations lead to variations of the antenna reflection coefficient, which can be measured. Visualization of obtained 2-D distribution of the reflection coefficient makes an image of subsurface inhomogeneities.

At first, the spectrum of the reflection coefficient for various subsurface structures under the surface of a human body has been studied. In Fig.2 one can see that different subsurface structures of living tissues have different response in the reflection. This fact makes it possible to use the reflection measurements for the microwave subsurface sounding. From results shown in Fig.2 one can conclude that the most suitable frequencies for the MW imaging can be chosen from the frequency range 1100-1140 MHz where the reflection difference for various tissues is more pronounced. It is reasonable to make measurements at near-zero values of the reflection coefficient for some place inside an area of measurements because it improves the accuracy and makes a high level of the image contrast.

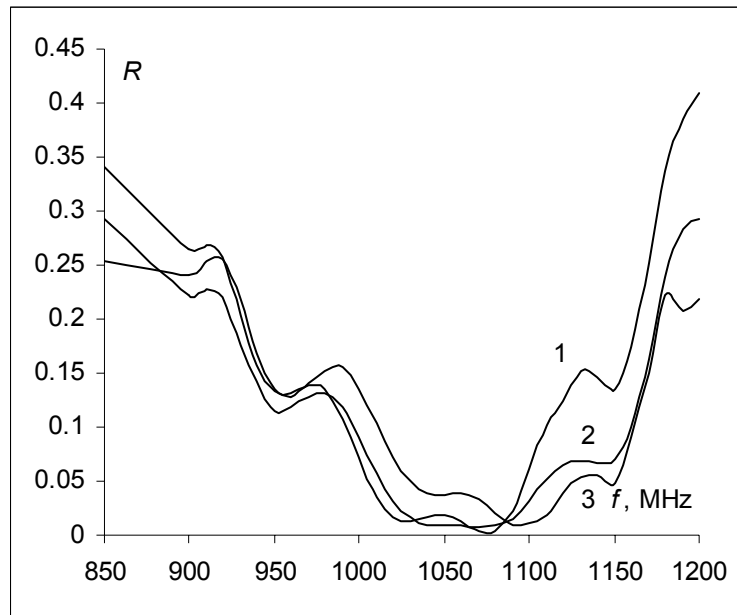
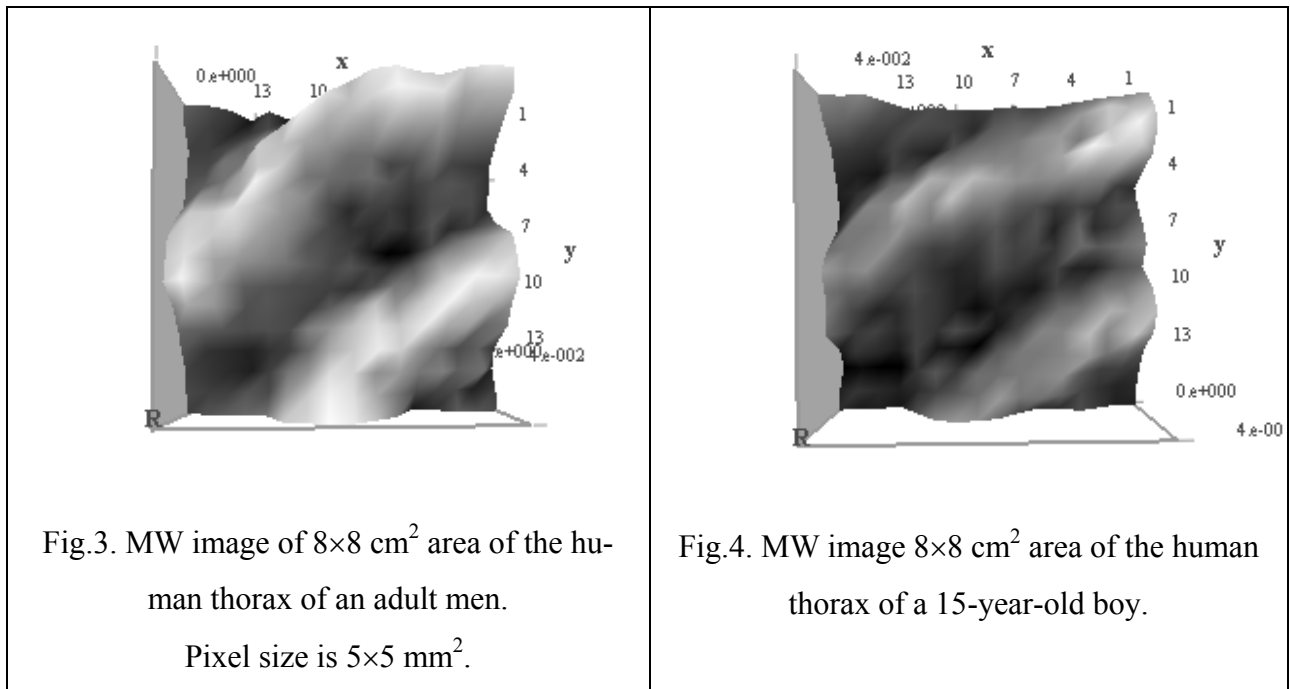


Fig.2. Reflection spectrum for living tissues. 1 – forehead, 2 – biceps, 3 – belly.

The frequency $f_0 = 1110$ MHz has been used for scanning in our measurements of living tissues. In Figs.3-4 results of MW imaging of the human thorax are shown.



It is possible to see that details of the subsurface structure of living tissues are clearly seen. In particular, one can see two ribs and inhomogeneities of the adjacent tissue structure for the cases of adult and young men. These results show possibilities of MW subsurface imaging of living tissues.

There are also problems that should be solved. First of all, it is necessary to build the automatic scanning system. It is not easy task because the antenna properties are very sensible

to small variations of inclination at the application. May be, antenna arrays can be used in this diagnostics.

Second, it is very interesting to retrieve the subsurface distribution of dielectric parameters. The effective depth of this active sounding is comparable to the antenna size; hence it allows the possibility to develop methods of subsurface dielectric structure sounding using the dependence of reflectivity on antenna size. Each antenna has typically more than one matching frequency – it opens the possibility of multi-frequency analysis. These approaches are inevitable related to the solution of very complicated electrodynamic problems.

The approach used in this paper is very similar with that in [2] where a microwave near-field system for the subsurface sounding of thin dielectric samples has been build. In [2] we also had a low enough space resolution as compared to the surface imaging in near-field scanning microscopy at microwave frequencies [3-4]. The high resolution in this kind of microscopy is achieved by decreasing of the probe size because the resolution is determined by this size. However, the increasing of resolution leads simultaneously to decreasing of the sounding depth because it is also about the probe size. Thus, a large penetration depth as an important advantage of microwave range is lost in microwave microscopy. In our subsurface microwave imaging we use larger antennas to achieve the necessary penetration depth (that is also comparable to the antenna size) but, of course, at the cost of resolution decrease. There is a difference between the approach used in this paper and methodic of [2]. We use here the wideband antenna (the band width ~ 150 MHz) instead of narrow-banded antenna (15 MHz) in [2]. The wide frequency range made it possible to optimize the wavelength selection in the approach presented here.

It is possible to conclude from the results of our study that the MW living tissues imaging has a good prospect, and it is much less harmful in comparison with the X-ray diagnostics. This method can be used also for the subsurface imaging of other dielectric media.

This work was supported by the RFBR, grant *No.*01-02-16432.

References

1. Gaikovich K.P., Reznik A.N., Vaks V.L., Yurasova N.V. Physical Review Letters, 11 March 2002, v.88, No.10, pp.104302-1 – 104302-4.
2. Gaikovich K.P., Yu.N.Nozdryn, A.N.Reznik, and V.L.Vaks. Physics of Low-Dimensional Structures, 2002, v.5/6, pp.99-104.
3. E.A.Ash, G.Nicholls. Nature, June 1972, v. 237, p.510.
4. T.Nozoekido et al. IEEE Trans. MTT, 2001, v.49, N3 p.491.